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A scalable synthesis of adjuvanting antigen depots based on metal–organic frameworks†

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Vaccines have saved countless lives by preventing and even eradicating infectious diseases. Commonly used subunit vaccines comprising one or multiple recombinant proteins isolated from a pathogen demonstrate a better safety profile than live or attenuated vaccines. However, the immunogenicity of these vaccines is weak, and therefore, subunit vaccines require a series of doses to achieve sufficient immunity against the pathogen. Here, we show that the biomimetic mineralization of the inert model antigen, ovalbumin (OVA), in zeolitic imidazolate framework-8 (ZIF-8) significantly improves the humoral immune response over three bolus doses of OVA (OVA 3×). Encapsulation of OVA in ZIF-8 (OVA@ZIF) demonstrated higher serum antibody titers against OVA than OVA 3×. OVA@ZIF vaccinated mice displayed higher populations of germinal center (GC) B cells and IgG1+ GC B cells as opposed to OVA 3×, indicative of class-switching recombination. We show that the mechanism of this phenomenon is at least partly owed to the metalloimmunological effects of the zinc metal as well as the sustained release of OVA from the ZIF-8 composite. The system acts as an antigen reservoir for antigen-presenting cells to traffic into the draining lymph node, enhancing the humoral response. Lastly, our model system OVA@ZIF is produced quickly at the gram scale in a laboratory setting, sufficient for up to 20 000 vaccine doses.

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Introduction

Edward Jenner discovered that the administration of cowpox blister fluid, which contained live cowpox virus, effectively prevented smallpox; these efforts established the modern field of vaccination and significantly reduced infectious disease-related mortality.^{1–3} Over time, vaccine formulations have evolved, with subunit vaccines emerging as a preferred option, owing to their enhanced safety profile compared to early formulations such as inactivated and live vaccines.^{4,5} Subunit vaccines comprise one or more proteins called antigens (Ag) isolated from a specific pathogen.⁶ However, these proteinaceous subunit vaccines—like most biomacromolecule-based drugs—are delicate and easily destroyed by environmental factors, requiring cold-chain transportation.^{7–9} Additionally,

they are often weakly immunogenic and need several doses—typically called boosters—to achieve and maintain complete immunity against the pathogen.^{10–13} To achieve high antibody titers and immune memory, many of today's modern vaccines require a prime-boost regimen, where one or more additional doses of vaccine are needed, even in formulations that use adjuvants.^{12,14} However, patient compliance decreases with the number of doses required.¹⁵ The distaste for needles and vaccine side effects deters patients from receiving additional doses, taking a significant toll on the idea of herd immunity.^{16–20} Recent work has shown that sustained release of an antigen from an injected “depot” over several days provokes a more robust immune response than repeat injections.^{21–23} This suggests that a continuous release of Ag from an injection should outperform several injections, thereby removing the need for follow-up doses.

The emergence of biomimetic mineralization of delicate biomaterials in a metal–organic framework (MOF) has allowed for the development of thermally and enzymatically protected biological material from numerous stressors.^{24–30} Recent work has shown that the biofriendly zeolitic imidazolate framework-8 (ZIF-8)-encapsulated vaccines promote a more robust immune response against viral nanoparticles or whole-cell bacteria when

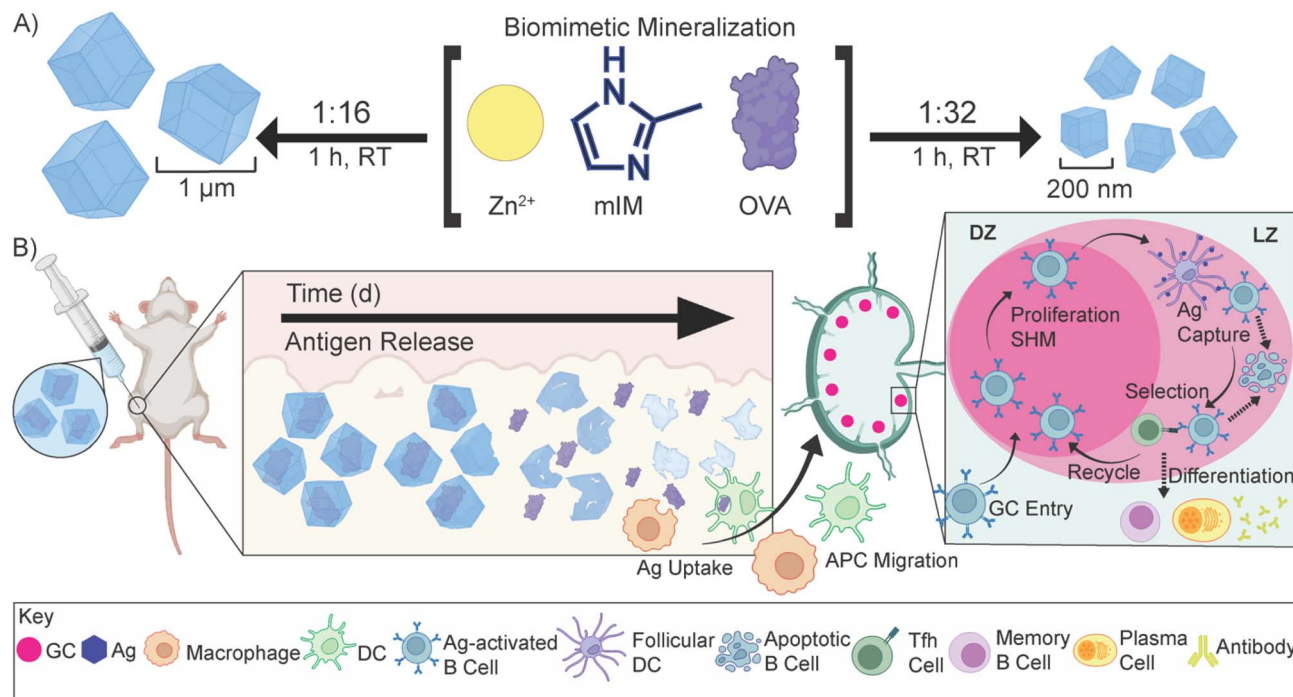
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Scheme 1 Biomimetic mineralization of OVA@ZIF and sustained release of antigens. (A) Synthetic scheme of μ -OVA@ZIF and n-OVA@ZIF. In a “one pot” reaction, Zn^{2+} , mIM, and ovalbumin are suspended in water and react for 1 h at room temperature. By adjusting the ligand-to-metal ratio, we can tune the size of these ZIFs. We formulated a 1 : 16, micron-sized ($\sim 1\ \mu\text{m}$) and 1 : 32 nano-sized ($\sim 200\ \text{nm}$) μ -OVA@ZIF and n-OVA@ZIF, respectively. (B) Sustained release of antigens following vaccination, allowing for the formation of GCs. The ZIF-8 crystals slowly degrade in the body, exposing the antigen to the immune system and allowing for a constant supply of antigen to the GC.

injected subcutaneously.^{24,25,31–33} These results are striking, but in all cases, the vaccines used have been “self-adjuncting” as the RNA or DNA within a virus or the lipopolysaccharides on the inactivated bacteria can induce their own strong immune response. Further, it is not clear what happens to the ZIF inside the skin, nor has size dependence on the toxicity of the particles *in vivo* been assessed as they reside for so long within the tissue.

This work details the MOF encapsulation of a model antigen, ovalbumin (OVA), in ZIF-8 (OVA@ZIF). By adjusting the metal-to-ligand ratio, we can adjust the size of our vaccine composites. We formulated nano- and micro-sized OVA@ZIF (n-OVA@ZIF) and (μ -OVA@ZIF), respectively (Scheme 1A). We show the process of MOF shell degradation within tissue over several days, which provides a constant supply of antigens to the immune system.^{34–36} This provokes a stronger immune response over bolus vaccine.³⁷ Constant supply of antigen through the depot effect promotes the formation of more developed germinal centers (GCs—Scheme 1B) within follicular lymph nodes.^{38–44} GCs are the location of B cell development, which is crucial for a strong and protective antibody response. Additionally, we show that, as the ZIF degrades, the draining lymph node has increased zinc concentrations. Zinc is known to promote immune activation, particularly in combination with an antigen, and so its presence in conjunction with the resulting robust immune response suggests the metal may be helping adjuvant the immune response. The resulting Ag release and ZIF dissolution from the ZIF depot promote GC development, resulting in a single injection of OVA@ZIF producing more

antibodies than three bolus injections of OVA (OVA 3 \times). Finally, we show that the synthesis of OVA@ZIF is easily scaled in the laboratory to multi-gram quantities.

Results and discussion

Synthesis and cytotoxicity

In a one-pot aqueous synthesis, OVA, 2-methyl imidazole (mIM), and Zn^{2+} react at room temperature for 1 h to form the OVA@ZIF composite through biomimetic mineralization—an *in situ* process where the protein templates nucleate the MOF crystal growth yielding total encapsulation of the protein within the ZIF-8 framework.^{45–47} By adjusting the metal-to-ligand ratios, we can tune the size of these composites; higher metal-to-ligand ratios tend to yield larger particles.⁴⁸ To investigate if size plays an important role in the compatibility of our system, we synthesized two formulations of OVA@ZIF. A 1 : 32 metal-to-ligand ratio yielded nano-sized particles approximately 200 nm in diameter n-OVA@ZIF, and a 1 : 16 metal-to-ligand ratio yielded micron-sized, approximately 1 μm μ -OVA@ZIF. Scanning electron microscopy (SEM) micrographs of both μ -OVA@ZIF and n-OVA@ZIF show approximately 1 μm and 200 nm crystals, respectively (Fig. 1A and B). Powder X-ray diffraction (PXRD) diffractograms confirm the crystallinity of both ZIF-8 formulations and the vaccine formulations μ -OVA@ZIF and n-OVA@ZIF (Fig. 1C). To help visualize release kinetics and study uptake *via* flow cytometry, cyanine-7 (Cy7) labeled OVA (OVA[Cy7]) were produced and encapsulated in



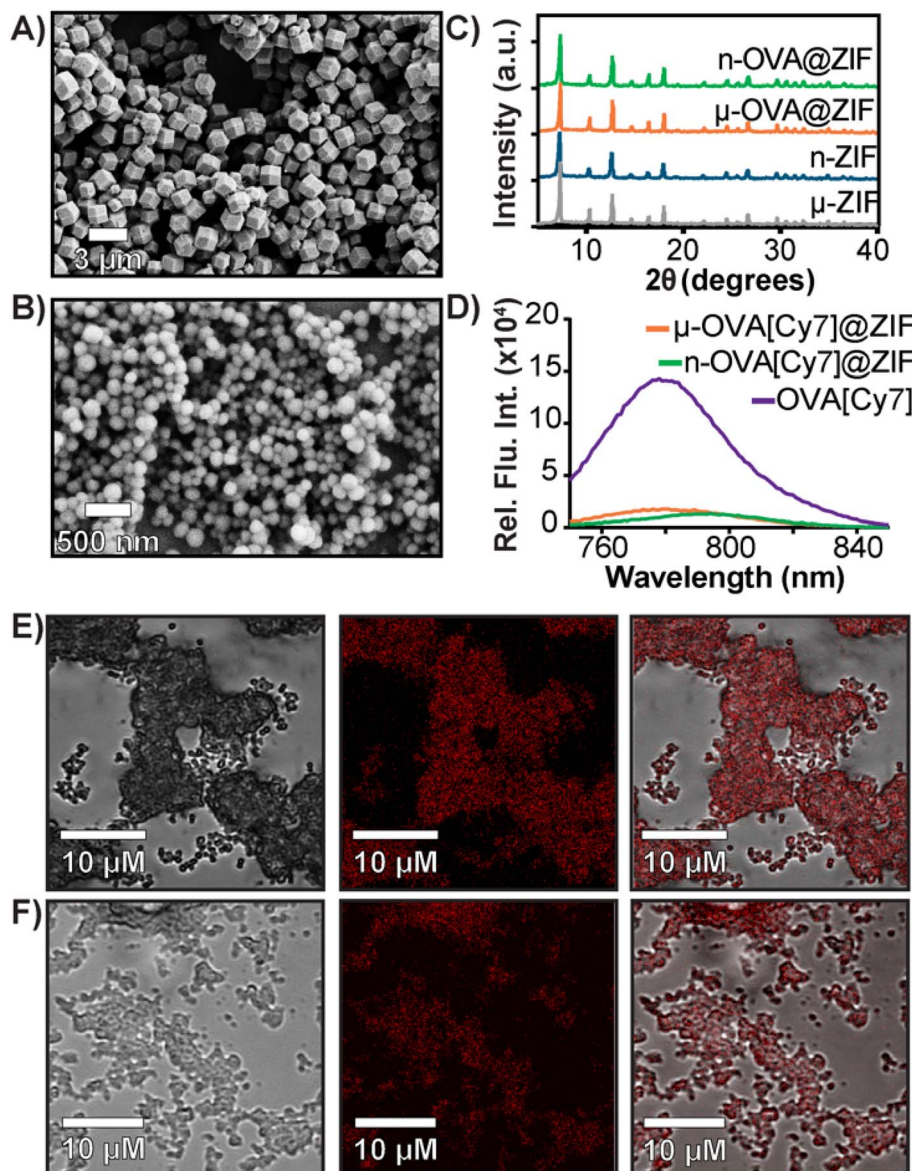


Fig. 1 Characterization of OVA@ZIF. (A) SEM images of μ -OVA@ZIF and (B) n-OVA@ZIF. (C) PXRD diffractogram of OVA@ZIF composites. (D) Encapsulation efficiency of μ -OVA[Cy7]@ZIF and n-OVA[Cy7]@ZIF as measured by Cy7 fluorescence in the supernatant ($\lambda_{\text{ex}} = 756$ nm and $\lambda_{\text{em}} = 779$ nm). (E) CLSM images of μ -OVA[Cy7]@ZIF and (F) n-OVA[Cy7]@ZIF. Brightfield images are shown on the left, fluorescent in the middle, and merged channels on the right.

both micro-sized (μ -OVA[Cy7]@ZIF) and nano-sized (n-OVA[Cy7]@ZIF) formulations using the previously mentioned formula. We used the fluorescence of the resulting supernatant to determine encapsulation efficiency (Fig. 1D). The encapsulation efficiency of both formulations was greater than 98%. μ -OVA[Cy7]@ZIF and n-OVA[Cy7]@ZIF crystals were imaged through confocal laser scanning microscopy (CLSM) to confirm that the fluorescence is due to the presence of OVA[Cy7]. CLSM images of non-labeled μ - and n-OVA@ZIF further confirm that the fluorescent intensity is from fluorophore-conjugated protein (Fig. S1 and S2[†]). The n-OVA@ZIF formulation has a lower drug loading ratio of 1:37 w/w ovalbumin to ZIF composite, as compared to μ -OVA@ZIF, which has a 1:28 w/w

drug loading ratio. The MOF in these ZIF composites maintains porosity and surface area in all ZIF formulations, as demonstrated in Fig. S3[†] by N_2 gas adsorption isotherms. As expected, the OVA@ZIF formulations have slightly reduced surface area as a portion of the mass is now made up of protein. Additional characterization, including X-ray photoelectron spectroscopy (XPS) and Fourier transform infrared (FT-IR) spectroscopy of all the ZIF formulations, can be found in Fig. S4 and S5,[†] respectively. These results further prove we have produced ZIF-8.

The safety and toxicology of ZIF-8 have been an area of substantial research;^{49–51} however, to the best of our knowledge, it has yet to be benchmarked against current FDA-approved



therapeutics. To that end, we conducted a study to compare ZIF-8 formulations against the adjuvant alum, which is nearing a century of use in vaccine formulations.⁵² The alum formulations that are typically used to adjuvant an immune response in humans consist of either aluminum hydroxide (alum(OH)) or aluminum phosphate (alum(PO₄)).⁵³ We conducted *in vitro* cytotoxicity comparisons between alum salts and our ZIF-8 formulations using lactate dehydrogenase (LDH) assay to assess the safety profiles. We utilized immortalized murine RAW 264.7 macrophages (Fig. 2A) as a standard lab-strain and primary bone marrow-derived macrophages (BMDMs) to represent more realistic toxicities in fresh primary cells. Remarkably, alum(OH) exhibited significant toxicity in both cell assays, while alum(PO₄) demonstrated higher toxicity in the BMDM assay than in the RAW 264.7 assay. Conversely, the μ -OVA@ZIF formulation showed no toxicity in either cell assay at tested concentrations, while n-OVA@ZIF displayed reduced cell viability in the RAW 264.7 assay without significant cytotoxicity in primary BMDMs. Overall, our results indicate that alum salts have a stronger toxic profile than our μ -OVA@ZIF formulation and are at least comparable with n-OVA@ZIF. This aligns with

existing literature,^{54,55} and our study provides evidence that ZIF-8 is a less toxic adjuvant than the FDA-approved alum. Thus, our findings establish that μ -OVA@ZIF is the least toxic among all tested materials. In addition, we assessed cellular uptake using flow cytometry in RAW 264.7 macrophages and found uptake of μ -OVA[Cy7]@ZIF to be statistically insignificant ($p = 0.09$) compared to n-OVA[Cy7]@ZIF, yet superior to naked OVA[Cy7] (Fig. 2B).

Tissue residency and time-dependent dissolution

To assess the tissue residency of our formulations, μ -OVA[Cy7]@ZIF, n-OVA[Cy7]@ZIF, and OVA[Cy7] (10 μ g of OVA[Cy7]) were subcutaneously injected into the right flank of female BALB/c mice ($n = 4$), and Cy7 fluorescence intensity was monitored over time through fluorescent live animal imaging (Fig. 3A and B). Fluorescence intensity in the OVA[Cy7] was significantly less than the OVA[Cy7]@ZIF cohorts at 24 h ($P \leq 0.001$ for both μ - and n-OVA[Cy7]@ZIF with respect to OVA[Cy7]), and the signal was completely diminished in the OVA[Cy7] cohort at 36 h. Whereas μ - and n-OVA[Cy7]@ZIF cohorts demonstrated a vastly longer tissue residency of Ag, with notable fluorescent signal

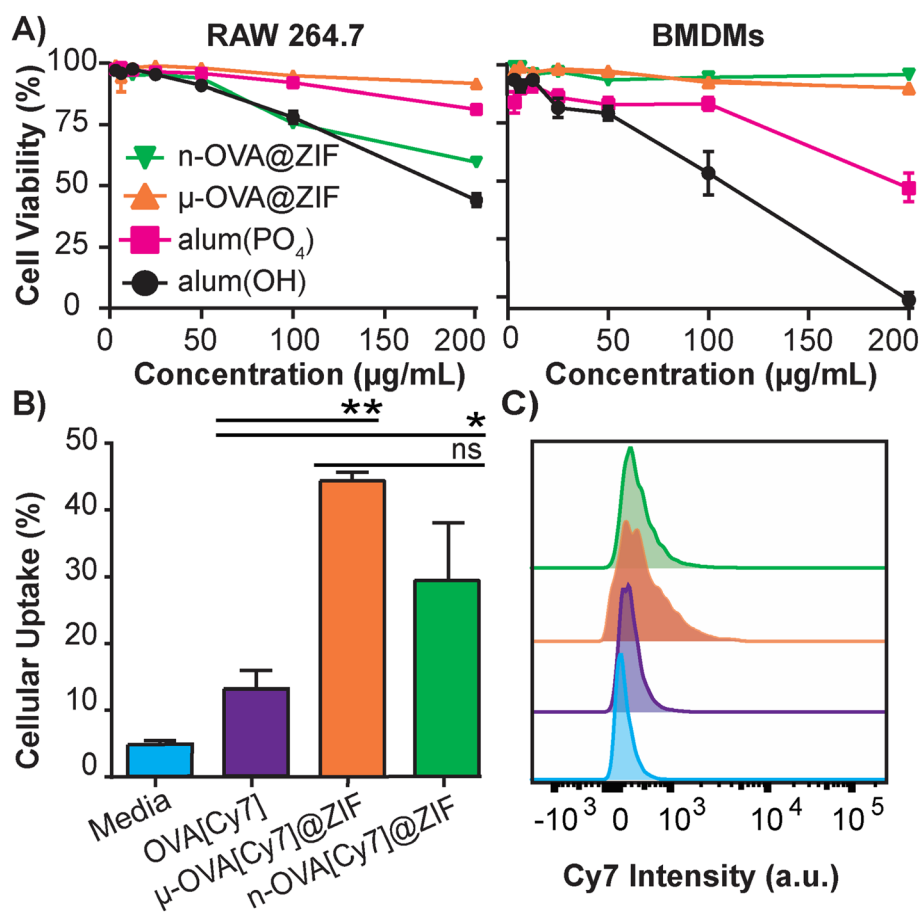


Fig. 2 *In vitro* studies of OVA@ZIF. (A) Cell viability after 4 h incubation of ZIFs and alum in immortalized RAW 264.7 cells (left) and primary BMDMs (right) using LDH assay. (B) Flow cytometry analysis of the cellular uptake of μ -OVA[Cy7]@ZIF and n-OVA[Cy7]@ZIF by RAW 264.7 macrophage following 4 h incubation. (C) Representative histogram overlay of flow cytometry plot illustrating the Cy7 intensity of RAW 264.7 macrophages following uptake experiment. Statistical significance was determined by an unpaired Student's *t*-test ($P > 0.05$ is ns, $P \leq 0.05$ is *, $P \leq 0.01$ is **, $P \leq 0.001$ is ***, and $P \leq 0.0001$ is ****).



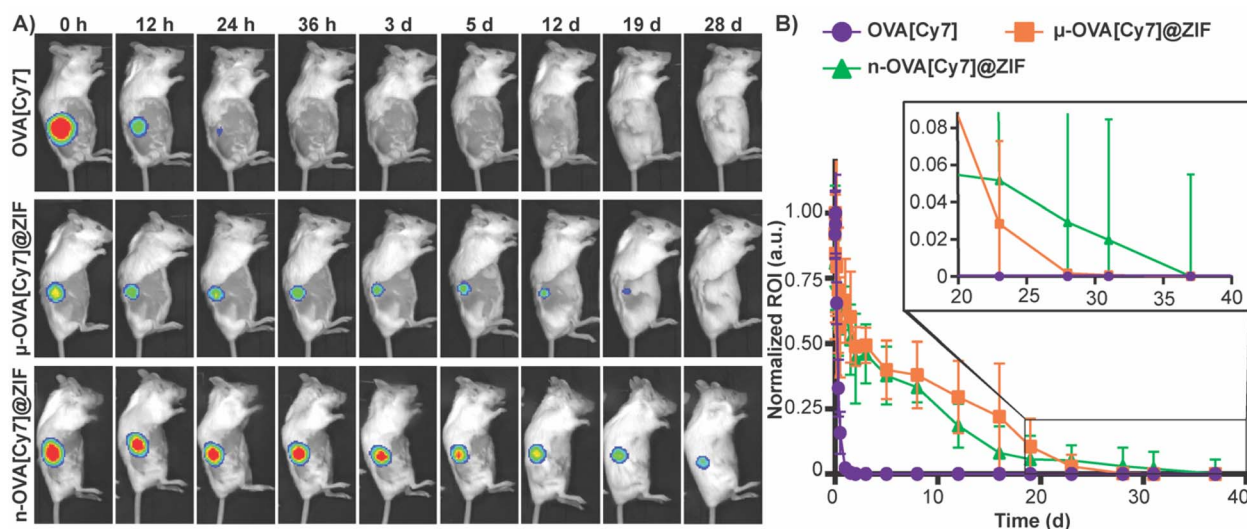


Fig. 3 Evaluation of μ -OVA@ZIF and n-OVA@ZIF tissue residency. (A) Representative images of Cy7 fluorescence in the right flank of mice subcutaneously injected with OVA[Cy7] (top), μ -OVA[Cy7]@ZIF (middle), and n-OVA[Cy7]@ZIF (bottom) (B) normalized Cy7 fluorescence from mice subcutaneously injected with OVA[Cy7], μ -OVA[Cy7]@ZIF, and n-OVA[Cy7]@ZIF (10 μ g OVA[Cy7]) over the course of 38 days ($n = 4$).

until day 28 and 31, respectively. It is worth noting that there is no statistical significance between μ - and n-OVA[Cy7]@ZIF at any of the reported time points ($P > 0.05$). In agreement with our hypothesis, OVA@ZIF shows significant enhancement of tissue residency of the Ag. However, the n-OVA[Cy7]@ZIF injected mice developed inflammation and skin irritation at the injection site (Fig. S6†). This is likely caused by the sub-micron size of the n-OVA@ZIF particles; previous literature suggests that these smaller particle sizes can cause nanotoxicity.^{56,57} In contrast, the μ -OVA[Cy7]@ZIF formulation showed no signs of *in vivo* toxicity and demonstrated a sustained release profile similar to the n-OVA[Cy7]@ZIF. We extracted the inguinal lymph node (ILN) closest to the injection site and the contralateral inguinal lymph node (CILN) on day 14 following a single dose of OVA, n-OVA@ZIF, and μ -OVA@ZIF. Saline was used as a negative control. Both μ -OVA@ZIF and n-OVA@ZIF should predominantly exert their immunological effect within the ILN as compared to the much more distant CILN. Consequently, we expect to see morphological changes—*e.g.*, enlargement—in the ILN as a result of the immune response compared to the CILN.^{58,59} Gross pathological examination found that μ -OVA@ZIF formulation produced the largest ILN, indicating that this formulation would encourage a more robust immune response (Fig. S7†). From these preliminary *in vivo* data, with both formulations demonstrating similar tissue residency times, we conclude that μ -OVA@ZIF is more biocompatible and appears to be more efficient at activating the immune system. Looking at both the *in vitro* and *in vivo* data, we decided that μ -OVA@ZIF was the preferred vaccine formulation and was therefore used in further experiments.

To qualitatively assess the degradation of ZIF-8 crystals, we injected 50 μ L of μ -OVA@ZIF into BALB/c mice ($n = 2$) (Fig. 4A). 24 h, 48 h, 72 h, and 96 h post-vaccination, the mice were euthanized, and ZIF-8 crystals were extracted from the injection site as a white bio-aggregate clump (Fig. S8†). SEM images were

taken of pristine and *ex vivo* ZIF-8 (Fig. 4B). It is known that ZIF-8 degrades in the presence of phosphates and albumin.³⁴ There was a definitive difference between pristine and *ex vivo* ZIF-8. After 24 h, some crystals maintained their rhombic dodecahedron shape, while others developed large cavitations. After 48 h, the crystals appeared to be majority amorphous in structure, and after 72 h, no obvious ZIF-8 crystals were seen in the SEM micrographs (Fig. 4B). At 96 h post-injection, we could no longer find crystals with the naked eye, though fluorescence data clearly show the presence of antigen. We thus conclude that the OVA@ZIF persists as micro or nanoparticles too small to see with the unaided eye. It is worth noting that we were able to extract less material with every successive time point.

The high concentration of metal in MOF carrier systems poses a challenge when translating these delivery systems to a clinical setting—thus far, only one MOF system has made it to phase I clinical trials.⁶⁰ To further understand the safety and metabolism of the MOF composites, we performed an *in vivo* study to quantify Zn^{2+} distribution to major organs. We vaccinated female BALB/c mice ($n = 3$) with μ -OVA@ZIF and following inoculation, major organs (including the ILN, the injection site, and the flank) were extracted after 24 h, 1 w, and 2 w post-vaccination. Inductively coupled plasma mass spectrometry (ICP-MS) was used to quantify zinc concentrations in organs. Our experimental design is represented by Fig. 5A. As a negative control, naïve mice ($n = 3$) were used as the baseline to determine typical Zn^{2+} concentrations in each organ. The spleen, a crucial organ of the lymphatic system, displayed no significant changes in metal concentration (Fig. 5B). Interestingly, the ILN, contained significantly more Zn^{2+} 24 h post-vaccination but returned to baseline by day 7 (1 w—Figure 5C). It has been known that maintaining homeostatic zinc levels is crucial for normal immune function.^{61,62} However, recent studies have shown that using zinc as a therapeutic has immunogenic properties, including T cell activation and IFN- γ production (a pro-inflammatory cytokine).^{63,64} This warrants



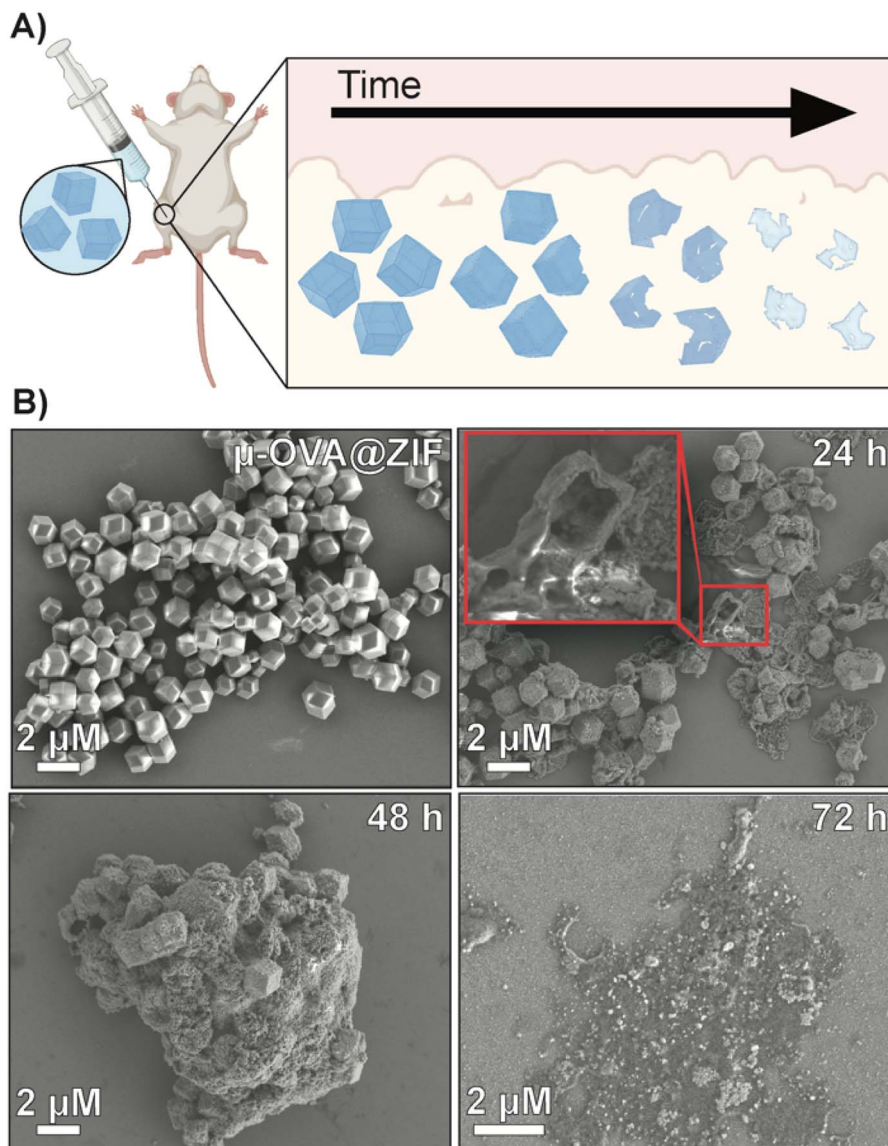


Fig. 4 Degradation analysis of μ -OVA@ZIF post-injection. (A) Schematic representation of the degradation of ZIF-8 crystals *in vivo*. (B) SEM images of pristine μ -OVA@ZIF and the *ex vivo* extracts at 24 h, 48 h, and 72 h post-injection.

further investigation into zinc's role in adjuvanting the vaccine@MOF. Like the ILN, the liver demonstrates a slight yet statistically significant increase in zinc concentration at 24 h but returns to baseline by 1 w (Fig. 5D). The kidneys, lungs, and heart presented no significant change in metal content compared to the negative control (Fig. 5E, F and H). The depot site, the flank, required two weeks to return to baseline; however, this is expected as we previously demonstrated that the μ -ZIFs reside at the injection site for at least 2 w as shown in Fig. 3.

Adjuvanting of ZIF-8 and germinal center development

The ability of ZIF-8 encapsulation to enhance the immune response against the model Ag, OVA, was evaluated *in vivo* by looking at the humoral response. Female BALB/c mice were injected with either three bolus injections of OVA or one dose of μ -OVA@ZIF ($n = 5$). The single dose and two subsequent

boosters delivered to each mouse contained 25 μ g of OVA, so OVA 3 \times received thrice the amount of Ag. Mice were injected with OVA on days 0, 7, and 14 to simulate a booster dose injection schedule. μ -OVA@ZIF was injected once on day 0. To investigate the long-term humoral immunity of single dose OVA@ZIF *versus* OVA 3 \times , total IgG was investigated from days 14 to 91 following the first administration of OVA@ZIF and OVA 3 \times (Fig. 6A). Using ELISA, endpoint titer total IgG was determined using saline mice as the baseline. There was higher anti-OVA IgG in the serum of single dose μ -OVA@ZIF *versus* OVA 3 \times across all time points (Fig. 6B).

We observed that zinc was being trafficked into the lymph node in the previous study illustrated by Fig. 5C. This prompted us to further investigate the role zinc may have in adjuvanting our vaccine@MOF. As previously mentioned, zinc has been shown to cause IFN- γ production and T-cell activation. To check



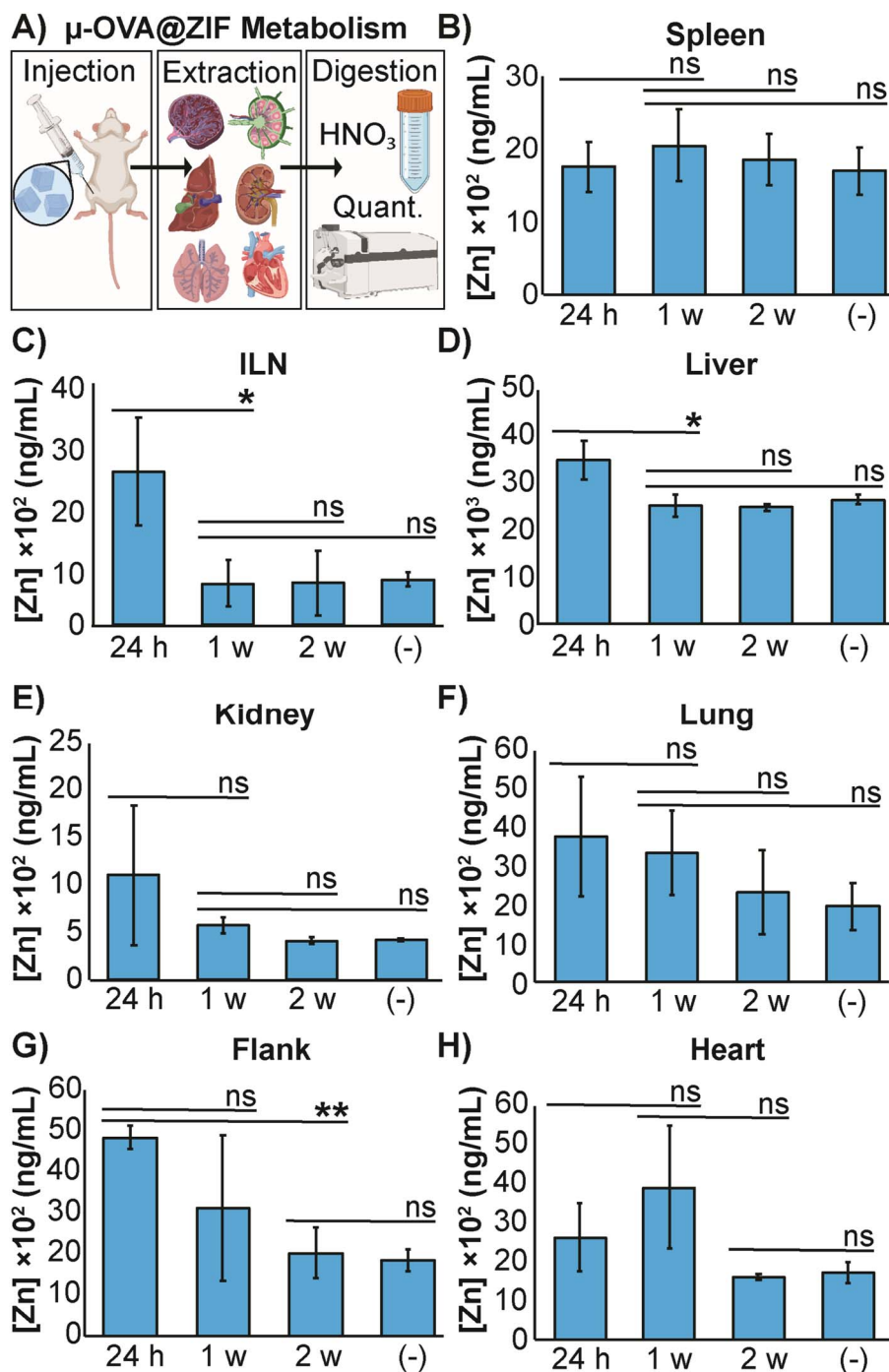


Fig. 5 Distribution of zinc released from μ -OVA@ZIF. (A) Representative scheme illustrating the vaccination, organ extraction, sample digestion, followed by quantification of Zn^{2+} through ICP-MS. The concentration of Zn^{2+} in the (B) spleen, (C) ILN, (D) liver, (E) kidneys, (F) lungs, (G) flank and (H) heart of female BALB/c mice ($n = 3$) following vaccination with μ -OVA@ZIF. Organs were extracted at 24 h, 1 w, and 2 w post inoculation. (–) denotes the negative control consisting of unvaccinated mice ($n = 3$). Statistical significance was determined by an unpaired Student's t -test ($P > 0.05$ is ns, $P \leq 0.05$ is *, $P \leq 0.01$ is **, $P \leq 0.001$ is ***, and $P \leq 0.0001$ is ****).

if our vaccine@MOF is inducing the production of the pro-inflammatory cytokine, $\text{IFN-}\gamma$, we determined the concentration of $\text{IFN-}\gamma$ in serum through ELISA on day 7 and day 14 following vaccination of naïve BALB/c mice ($n = 5$) with saline (negative control), bolus OVA, and μ -OVA@ZIF. There was no significant difference between the negative control and bolus

OVA. However, as we suspected, there was significantly higher concentration of $\text{IFN-}\gamma$ in serum taken from the μ -OVA@ZIF cohort on both day 7 (Fig. 6C) and day 14 (Fig. 6D). This prompted us to further investigate the role ZIF alone plays in promoting the activation of T cells, specifically CD4^+ T helper cells. Here, we vaccinated BALB/c mice ($n = 8$ saline, $n = 9$ μ -ZIF)



Fig. 6 Humoral response of single dose μ -OVA@ZIF vs. OVA 3 \times . (A) Scheme of vaccine and blood draw schedule for determining endpoint titers of anti-OVA IgG. (B) Endpoint titers of Anti-OVA IgG from mouse serum. IFN- γ concentration (pg mL⁻¹) in mouse serum following vaccination on (C) day 7 and (D) day 14 determined through ELISA. (E) Day 21 GC formation in the ILN of vaccinated mice. (F) Percentage of IgG1+ GC B cells in the ILN. Statistical significance was determined by an unpaired Student's *t*-test ($P > 0.05$ is ns, $P \leq 0.05$ is *, $P \leq 0.01$ is **, $P \leq 0.001$ is ***, and $P \leq 0.0001$ is ****).

with saline or μ -ZIF formulation—no antigen was present. After 72 h, the ILN was extracted and analyzed for CD4+ T effector cells through immunophenotyping *via* flow cytometry. CD4+ T effector cells, also known as T helper cells, are required for “helping” or activating immune cells involved in the adaptive immune system including B cells and CD8+ cytotoxic T cells. We observed significantly higher populations of CD4+ T eff cells in the ILN of μ -ZIF vaccinated mice in the ILN 72 h post-vaccination with respect to the negative control, saline (Fig. S9†). This discovery further supports our hypothesis that the presence of zinc in our vaccine@MOF is helping to promote an immune response, ultimately adjuvanting our vaccine.

GCs are crucial for successful immunization and immune memory, yielding antibody-producing plasma cells and long-lived memory B cells.⁶⁵ GCs form in secondary lymphoid tissues, such as lymph nodes, typically after 14–28 days following Ag exposure.⁶⁶ Ag-activated B cells enter the GC in what is known as the light zone (LZ) and undergo proliferation and rounds of somatic hypermutation (SHM), creating diverse clones of themselves. This diverse library of GC B cells will migrate to the dark zone (DZ) and begin affinity maturation where greater affinity antibodies are selected.^{67,68} GC B cells interact with follicular dendritic cells (DC) and T follicular helper cells (Tfh). Cells that “pass” the selection process will either differentiate into long-lived memory B cells or antibody-producing plasma cells or will return to the LZ and begin this process again. We observed higher populations of GC B cells on day 21 in the ILN of the μ -OVA@ZIF cohort compared to OVA 3 \times (Fig. 6E). Memory B cells and plasma B cells arise from these GC, creating long-term immune memory and increased antibody production. We observe higher antibody titers in the μ -OVA@ZIF cohort until day 91, validating our hypothesis. Additionally, we observed higher IgG1+ GC B cells in the ILN of the μ -OVA@ZIF; this is indicative of class-switching recombination (CSR), a process where B cells begin to produce higher affinity antibodies (Fig. 6F). GC formation and CSR are two crucial benchmarks for assessing a vaccine's efficacy, as immune memory, long-term antibody production, and high-affinity antibodies are needed to maintain humoral immunity. The sustained release of the Ag by encapsulation in MOF provides a constant source of Ag, better equipping the immune system than three bolus injections of Ag. Additionally, hematoxylin and eosin (H&E) staining of tissue samples collected on day 21 show no significant sign of inflammation, tissue damage, or major morphological changes compared to saline (Fig. S10†). The gating strategy used to determine cell populations for Fig. 6E and F is shown in Fig. S11.†

Scalable synthesis

Finally, to demonstrate our formulation's ease of preparation and scalability, we synthesized the μ -ZIF formulations under the same conditions previously mentioned—we increased the volumes and concentrations. We made 2 L of μ -ZIF (Fig. 7A and B) and bovine serum albumin@ZIF (μ -BSA@ZIF) (Fig. 7A and B). We encapsulated 500 mg of BSA[Cy-7] (250 μ g mL⁻¹) in the 2 L ZIF-8 reaction. The reaction was left for 1 h on the benchtop



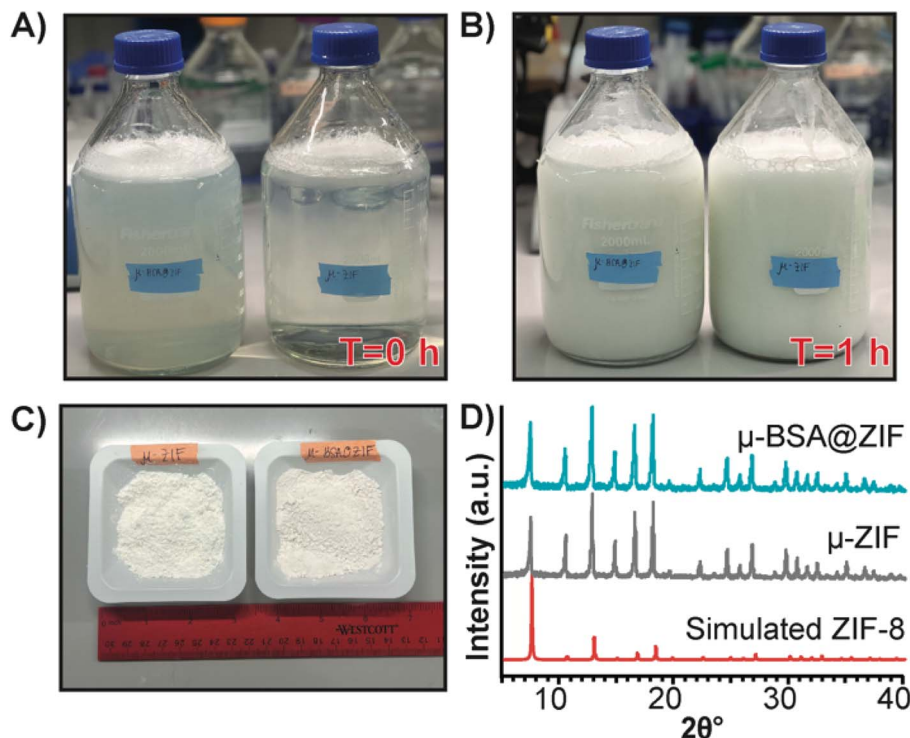


Fig. 7 Scaled synthesis of μ -ZIF and μ -BSA[Cy7]@ZIF. (A) Image of 2 L bottles (left: μ -BSA@ZIF, right: μ -ZIF) used for scaled-up ZIF synthesis at $T = 0$ h and (B) at $T = 1$ h. (C) 15.9 g of μ -ZIF powder (left) and 16.4 g μ -BSA[Cy7]@ZIF powder (right) from 2 L synthesis. (D) PXRD diffractograms of μ -BSA[Cy7]@ZIF (top), μ -ZIF (middle), and simulated ZIF-8 (bottom) following scaled synthesis.

(Fig. 7B). The encapsulation efficiency was $98.1\% \pm 1.64$, comparable to that of the 1 mL reaction of OVA@ZIF. Following a series of washes, the MOFs were dried under a vacuum, and the total weight of μ -ZIF was determined to be 15.9 g (Fig. 7C), and the drug loading ratio of albumin to ZIF is 1:32 w/w albumin to ZIF. The drug loading of the scaled reaction is similar to that of the 1 mL reaction (1:30 w/w) as we would suspect. We used BSA in this case because Ag-grade OVA is expensive, and it would be wasteful to create such a large batch of OVA@ZIF as no lab could possibly use this much material. It is worth mentioning, however, that Ag doses given to mice are typically the same as those given to humans (between 5–50 μ g per dose).^{12,69} This is the equivalent of 20 000 injections. Thus, this synthesis would prepare enough injections for a small town in an hour. PXRD diffractograms were obtained, and the sodalite crystallinity of both μ -BSA@ZIF and μ -ZIF was confirmed (Fig. 7D).

Conclusion

ZIF-8 has been found to be highly effective in improving the stability and protection of proteinaceous vaccine formulations against thermal and enzymatic degradation. In addition, it has been demonstrated that ZIF-8 can boost the immune response generated by the vaccine, to the extent that it can overcome the need for a three-series booster regimen. In terms of the humoral immune response, μ -OVA@ZIF has shown significantly higher levels of serum antibody titers against OVA as compared to

three bolus Ag doses. Not only does ZIF-8 encapsulation generate a strong immune response, but it also uses less antigen than the bolus injection. ZIF-8 encapsulation can reduce the number of needle injections and the amount of expensive, precious biomaterial. Lastly, we determined that this synthesis is easily scaled to a 2 L reaction volume while maintaining the short reaction time (1 h) and high encapsulation efficiency of protein (98%). We discovered that ZIF-8 possesses robust adjuvant properties and is less toxic than FDA-approved adjuvants like alum. Our research also indicates that zinc may play a role in promoting adjuvant activity, which is interesting and could provide considerable impetus to evaluate other MOFs as metalloimmuno-adjuvants. Zinc is known to encourage T cell maturation and the production of IFN- γ , which aligns with our findings of zinc trafficking into the lymph nodes through the metabolism of ZIF-8. These findings warrant further investigation into the role of zinc in ZIF-8's adjuvant properties to understand better and exploit this MOF-based delivery system.

Methods

Chemicals

Zinc acetate (ZnOAc), 2-methyl imidazole, sodium chloride, phosphate buffer saline (PBS) pH 7.4, Dulbecco's Modified Eagle Medium (DMEM), penicillin-streptomycin, L-glutamine, BSA, Ethylenediaminetetraacetic acid (EDTA), sodium bicarbonate (NaCO_3), dimethyl sulfoxide (DMSO), goat anti-mouse IgG (whole molecule)-alkaline phosphatase, magnesium



chloride (MgCl_2), paraformaldehyde (PFA) *p*-nitrophenyl phosphate (pNPP), tween-20, polyvinyl pyrrolidone (PVP), diethanolamine, potassium phosphate dibasic, potassium phosphate monobasic, hydrochloric acid, and sodium hydroxide were purchased from Sigma Aldrich (St. Louis, MO, USA) or Thermofisher Scientific (Waltham, MA, USA) and used without further modification. FBessence was purchased from VWR (Radnor, PA, USA). LDH assay, cell staining buffer (CSB), Zombie Red, Zombie UV, anti-mouse CD19 Alex Fluor 700 (AF700), anti-mouse IgG1 phyco-erythrin (PE), anti-mouse CD95 allophycocyanin (APC), and anti-mouse GL7 Alexa Fluor 488 (AF488) were purchased from Biolegend (San Diego, CA, USA). Vaccine-grade, endotoxin-free OVA was purchased from Invitrogen (Waltham, MA, USA) and Worthington Biochemical (Lakewood, NJ, USA). Bradford protein assay was purchased from BioRad Laboratories (Hercules, CA, USA). Non-fluorescent mouse diet was purchased from Lab Supply (Northlake, TX, USA). Cyanine 7-NHS (Cy7-NHS) was purchased from Lumiprobe (Cockeysville, MD, USA) and synthesized (Fig. S8–19†).

Instruments

SEM micrographs were taken on Zeiss Supra 40. PXRD patterns were obtained from Rigaku SmartLab X-ray diffractometer. XPS spectra was obtained on Versaprobe II scanning XPS. FT-IR spectra was obtained on Agilent Cary 660 FT-IR. Absorbance and fluorescence spectra were obtained on Biotek Synergy H4 Hybrid microplate reader. Thermofisher Scientific Sorvall Legend Micro17, Thermofisher Scientific Sorvall Lynx 4000, and Beckman Coulter Allegra X-14R centrifuges were used for obtaining cell and ZIF-8 pellets. CLSM images were taken on Olympus FV3000 RS microscope. The concentration of Zn in the extracted organs was quantified using Agilent 7900 ICP-MS. Flow cytometry data were acquired on a BD LSRFortessa. Cell counting was carried out on a Thermo Countess II. Live animal imaging was performed on an IVIS Lumina III. Paraffin embedding was done on Histo-Core ARCADIA. Embedded tissues were processed with a Leica RM22335 microtome. H&E images were obtained on VS120 virtual slide microscope. Ultrapure water was filtered in lab with the ELGA PURELAB flex 2 system.

Animals and ethics

Female BALB/c mice (4–6 weeks) were purchased from Charles Rivers Laboratories (Wilmington, MA, USA). *In vivo* experiments were approved by the University of Texas at Dallas Institutional Animal Care and Use Committee. This work was diligently carried out in accordance with protocol #19-06.

ZIF-8 synthesis

1 M ZnOAc and 3 M mIM stocks were made in sterile water (filtered and autoclaved). The final stock solutions were filtered through a 0.22 μm syringe filter. All microscale reactions took place at a final volume of 1 mL. For the nano-sized MOFs, sterile water, ovalbumin (150 $\mu\text{g mL}^{-1}$ in water), 2560 mM mIM, and 80 mM ZnOAc were added sequentially, vortexing after each addition. For the micro-sized MOFs, sterile water, OVA (150 $\mu\text{g mL}^{-1}$), 640 mM mIM, and 40 mM ZnOAc were added

sequentially, vortexing after each addition. The reaction vial was left for 1 h at RT. The resulting crystals were washed $3\times$ by centrifuging at $17\,000\times g$ for 5 min. The supernatant was removed, and the pellet was resuspended in 1 mL of sterile water.

Fluorescent labeling of protein

For OVA[Cy7], 10 mg mL^{-1} OVA was dissolved in 1 mL of 0.1 M NaCO_3 (pH 8.3). 63 μL of Cy7-NHS in DMSO dye solution was added to the OVA solution and vortexed well. The protein-dye solution was incubated overnight on a rotisserie at 4 $^\circ\text{C}$. The solution was washed with water in a 10 kDa protein concentrator at $4000\times g$ for 10 min until the filtrate was clear. The concentration of protein was determined through Bradford protein assay.

For BSA[Cy7] 1 g of BSA dissolved in 0.1 M NaCO_3 (pH 8.3). 1 mg of synthesized Cy7-NHS was dissolved in 200 μL of DMSO. The Cy7-NHS was added to the protein solution and vortexed well. The protein-dye solution was incubated overnight on a rotisserie at 4 $^\circ\text{C}$. The solution was washed with water in a 10 kDa protein concentrator at $4000\times g$ for 10 min until the filtrate was clear, indicating that the free Cy7 dye was removed. The concentration of protein was determined through Bradford Protein Assay.

Cell culture

RAW 264.7 murine macrophages were cultured in DMEM supplemented with 1% L-Glutamine, 2% penicillin-streptomycin, and 10% FBessence in a 75 cm^2 culture flask. Cells were grown at 37 $^\circ\text{C}$ with 5% CO_2 . Cells were passaged at 80–95% confluency by removing media, rinsing with 0.1 M PBS, followed by an additional 0.1 M PBS, and detaching cells with a cell scraper. The cell solution was centrifuged at $300\times g$ for 2 min.

Cytotoxicity

The night before, 1×10^5 viable RAW 264.7 cells were seeded in a 96-well plate in supplemented DMEM. Old media was aspirated. OVA, μ - and n-OVA@ZIF samples were diluted in complete DMEM and added to wells at a final volume of 100 μL . The cells were incubated with samples for 4 h at 37 $^\circ\text{C}$ with 5% CO_2 . Following the protocol from the LDH assay kit, 20 μL of lysis buffer was added to the high control and left to incubate for an additional 20 min at 37 $^\circ\text{C}$ with 5% CO_2 . Then, 100 μL of the working solution was added to each well and left to incubate in the dark for 20 min. 50 μL of stop solution was added, and the absorbance was read at 490 nm. Cell viability was determined through the following equation:

$$1 - \left(\frac{\left(\frac{\text{abs. of test substance} - \text{abs. low control}}{\text{abs. high control} - \text{abs. low control}} \right) \times 100 \right)$$

In vitro uptake

For uptake studies, 1×10^6 cells were added to a 24-well plate with 2 μg OVA[Cy7], 8 μL of μ - and n-OVA[Cy7]@ZIF (2 μg OVA). The cells were incubated with samples for 4 h at 37 $^\circ\text{C}$ with 5% CO_2 . The cells were washed $3\times$ with 0.5 M EDTA and $3\times$ with



PBS. Cells were stained with a 1 : 2000 zombie red solution in PBS for 20 min on ice and in the dark. Cells were centrifuged and resuspended in CSB (0.1 M PBS, 5% FBS, 0.5 mM EDTA, and 2 mM NaN₃). Flow cytometry analysis was performed on a BD LSRFortessa flow cytometer, and 100 000 events were recorded. Raw data were processed and analyzed using FlowJo software. Dead cells were gated out by selecting the negative zombie red population, and Cy7 positive cells were assumed to have uptake OVA. The Histogram overlay was normalized to mode.

Tissue residency

12 female BALB/c ($n = 4$) mice were fed a non-fluorescent diet for at least 48 h before the start of the experiment. The day before vaccination, mice were depilated with Nair hair remover on the side of the injection. Mice were anesthetized with isoflurane before injections or imaging. Baseline images of each mouse were obtained before the injection of the sample. OVA [Cy7], μ -OVA[Cy7]@ZIF, and n-OVA[Cy7]@ZIF (10 μ g OVA per dose) were injected subcutaneously with the sample into the right flank of each mouse. Mice were imaged at $t = 0$ h, 0.5 h, 1 h, 2 h, 4 h, 8 h, 24 h, 36 h, 2 d, 3 d, 5 d, 8 d, 12 d, 16 d, 19 d, 23 d, 28 d, 31 d, and 37 d. Data were normalized using GraphPad Prism.

Ex vivo degradation

100 μ L of μ -OVA@ZIF in 0.1 M saline was injected into both flanks (to increase the chance of retrieving the sample) of female BALB/c mice ($n = 2$). Mice were euthanized through cervical dislocation, and samples were removed from the subcutaneous layer at 24, 48, 72, and 96 h (no sample was found at 96 h). Samples were washed 3 \times with water.

Ex vivo organ Zn concentration determination

100 μ L of μ -OVA@ZIF in 0.1 M saline was subcutaneously injected into the left flank of female BALB/c mice ($n = 3$). At 24 h, 1 w, and 2 w. Mice were euthanized *via* cervical dislocation, and major organs (including flank, ILN, kidneys, lungs, liver, and spleen) was removed post-mortem. A negative control of naïve mice ($n = 3$) was used to determine the baseline concentration of Zn in the previously mentioned organs. Organs were first digested in 70% nitric acid. Then the digested organs were diluted to 35% nitric acid and syringe-filtered with a 0.22 μ m filter. The filtered solution was finally brought up to a concentration of 2% nitric acid using ultra-pure water. Commercially available Zn standards were used for determination of the Zn concentration.

T cell activation

Female BALB/c ($n = 8$ or $n = 9$) were subcutaneously vaccinated with 100 μ L of 0.1 M saline or μ -ZIF in the left flank. After 72 h, the mice were sacrificed *via* cervical dislocation and the ILN was extracted and homogenized with a mortar and 100 μ M cell strainer. Lymphocytes were stained with an antibody cocktail (anti-CD3, anti-CD4, anti-CD44, and anti-CD62L) for 1 h in the

dark and on ice. Cells were washed and flow cytometry was performed to determine the percent population of T eff cells.

In vivo antibody production

Female BALB/c mice ($n = 5$) were vaccinated subcutaneously with three doses of 100 μ L 0.1 M saline and 100 μ L OVA (75 μ g OVA total) on days 0, 7, and 14. Additionally, one dose of μ -OVA@ZIF (25 μ g OVA) on day 0. Mice were anesthetized with isoflurane, and blood was drawn weekly from day 14 until day 98. The serum was isolated by centrifuging blood samples at 1200 $\times g$ for 10 min to remove red blood cells. Serum was stored at -20 $^{\circ}\text{C}$ until further use.

Endpoint titer anti-OVA IgG ELISA

96-well Nunc titer plate was coated the night before with 100 μ L 1 μ g mL⁻¹ OVA in coating buffer (0.05 M NaCO₃ buffer pH 9.6). The plate was left to incubate overnight at 4 $^{\circ}\text{C}$. Plate was washed 4 \times with 300 μ L of wash buffer (0.1 M PBS 0.05% w/v tween-20 pH 7.4). The plate was blocked with 200 μ L of assay diluent (1% BSA in wash buffer) for 1 h at 37 $^{\circ}\text{C}$. The plate was washed 5 \times with wash buffer, and 100 μ L of serially diluted serum (100 \times –3200 \times) in assay diluent was added to each well. The plate was incubated at 37 $^{\circ}\text{C}$ for 1.5 h. The plate was subsequently washed 4 \times with wash buffer, followed by the addition of 100 μ L of (1 : 2000) alkaline phosphatase-conjugated goat anti-mouse IgG in conjugate buffer (0.02 g of PVP mL⁻¹ assay diluent). The plate was incubated at 37 $^{\circ}\text{C}$ for 1 h. The plate was incubated at 37 $^{\circ}\text{C}$ for 1 h. The plate was washed 4 \times with wash buffer. 100 μ L of 1 mg mL⁻¹ pNPP in substrate buffer (1 M diethanolamine buffer, 0.5 mM MgCl₂ pH 9.8) was added to the plate and left in the dark to incubate for 15 min or until color developed. Absorbance was read at 450 nm at 15 and 30 min. The endpoint titer was determined by plotting the dilution factor against 450 nm absorbance. The logarithmic curve was fit, and the endpoint titer was determined by the intersection of logarithmic fit to the average baseline (saline).

In vivo GC study

Female BALB/c mice ($n = 5$) were vaccinated subcutaneously with three doses of 100 μ L 0.1 M saline and 100 μ L OVA (75 μ g OVA total) on days 0, 7, and 14. Additionally, one dose of μ -OVA@ZIF (25 μ g OVA) on day 0. Mice were anesthetized before vaccination. On day 21, mice were euthanized *via* cervical dislocation, and the ILN was extracted along with other major organs (heart, lung, liver, and kidney) for H&E staining. A single-cell suspension was obtained by carefully passing cells through a 100 μ m cell strainer. Cells were washed 1 \times with 0.1 M PBS, resuspended in 1 mL of 0.1 M PBS, and counted using trypan blue to determine live/dead cells. Cells were stained with Zombie UV (1 : 2000) in 0.1 M PBS for 30 min on ice in the dark. Subsequently, the antibody cocktail (anti-mouse CD19 AF700, anti-mouse IgG1 PE, anti-mouse CD95 APC, and anti-mouse GL7 AF 488 in CSB) was added to the cells. The cells were left to stain for 30 minutes on ice in the dark. Cells were washed 3 \times with FACS buffer. Flow cytometry analysis was carried out on



a BD LSRFortessa flow cytometer. Raw data were processed and analyzed using FlowJo software.

H&E

Organs were incubated in 4% PFA for 48 h at ambient T on a shaker. Tissues were washed 3× with 0.1 M PBS, placed into tissue cassettes, and then into 70% ethanol. The organs were embedded in paraffin wax. Each organ was sectioned into 5 µm section using a rotary microtome. The sections were collected and stained with H&E for pathological analysis.

Scaled ZIF-8 synthesis

2 L of µ-ZIF was synthesized by adding 640 mM mIM, 40 mM ZnOAc, bringing the final volume to 2 L with MilliQ water. 2 L of µ-BSA[Cy7]@ZIF was synthesized by 640 mM mIM, 40 mM ZnOAc, 500 mg of BSA[Cy7]. The reaction bottles were vigorously shaken after adding the precursors and left to incubate for 1 h at ambient T. Solutions were transferred to 1 L centrifuge bottles and centrifuged for 30 min at 17 000 × g. The supernatant was discarded, and ZIF was resuspended in 200 mL of water, transferred to 50 mL disposable centrifuge tubes, and washed 2× with water. Tubes were then placed under a vacuum for drying.

Data availability

Raw and processed data used to create figures and displayed in the ESI† can be accessed at OSFHome at the following: <https://doi.org/10.17605/OSF.IO/7MHQU>.

Author contributions

Conceptualization: J. J. G. Methodology: R. N. E., O. R. B., Y. H. W., S. Kumari, F. C. H., investigation: R. N. E., O. R. B., Y. H. W., S. Kumari, I. T., O. T., T. S. H., F. C. H., A. R., S. Koirala, N. T., N. M. A., W. T., M. C. S., L. M. H. Manuscript preparation: R. N. E. and J. J. G.

Conflicts of interest

The authors declare no competing interests.

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References

- 1 D. A. Henderson, *Public Health Rep.*, 1997, **112**, 116–121.
- 2 S. A. Plotkin, *Nat. Med.*, 2005, **11**, S5–S11.
- 3 P. Pezzotti, S. Bellino, F. Prestinaci, S. Iacchini, F. Lucaroni, L. Camoni, M. M. Barbieri, W. Ricciardi, P. Stefanelli and G. Rezza, *Vaccine*, 2018, **36**, 1435–1443.
- 4 P. M. Moyle and I. Toth, *ChemMedChem*, 2013, **8**, 360–376.
- 5 A. Vartak and S. J. Sucheck, *Vaccines*, 2016, **4**, 12.
- 6 M. Hansson, P.-A. k. Nygren and S. Ståhl, *Biotechnol. Appl. Biochem.*, 2000, **32**, 95–107.
- 7 R. P. Welch, H. Lee, M. A. Luzuriaga, O. R. Brohlin and J. J. Gassensmith, *Bioconjugate Chem.*, 2018, **29**, 2867–2883.
- 8 R. Riccò, W. Liang, S. Li, J. J. Gassensmith, F. Caruso, C. Doonan and P. Falcaro, *ACS Nano*, 2018, **12**, 13–23.
- 9 D. M. Matthias, J. Robertson, M. M. Garrison, S. Newland and C. Nelson, *Vaccine*, 2007, **25**, 3980–3986.
- 10 M. Heidary, V. H. Kaviar, M. Shirani, R. Ghanavati, M. Motahar, M. Sholeh, H. Ghahramanpour and S. Khoshnood, *Front. Microbiol.*, 2022, **13**, 927306.
- 11 J. Poorolajal, M. Mahmoodi, R. Majdzadeh, S. Nasserimoghaddam, A. Haghdooost and A. Fotouhi, *Vaccine*, 2010, **28**, 623–631.
- 12 S. B. Manoff, S. L. George, A. J. Bett, M. L. Yelmene, G. Dhanasekaran, L. Eggemeyer, M. L. Sausser, S. A. Dubey, D. R. Casimiro, D. E. Clements, T. Martyak, V. Pai, D. E. Parks and B.-A. G. Collier, *Vaccine*, 2015, **33**, 7126–7134.
- 13 Y. Liao, Y. Chen, B. Chen, Z. Liang, X. Hu, B. Xing, J. Yang, Q. Zheng, Q. Hua and C. Yan, *Front. Immunol.*, 2022, **13**, 1017590.
- 14 É. Racine, V. Gilca, R. Amini, M. Tunis, S. Ismail and C. Sauvageau, *Vaccine*, 2020, **38**, 6205–6214.
- 15 C. B. Bridges, T. L. Watson, N. P. Nelson, M. Chavez-Torres, P. Fineis, B. Ntiri-Reid, E. Wake, J. M. Leahy, A. K. Kurian, M. A. K. Hall and E. D. Kennedy, *Vaccine*, 2019, **37**, 5111–5120.
- 16 A. Taddio, M. Ipp, S. Thivakaran, A. Jamal, C. Parikh, S. Smart, J. Sovran, D. Stephens and J. Katz, *Vaccine*, 2012, **30**, 4807–4812.
- 17 J. C. Nelson, R. C. L. Bittner, L. Bounds, S. Zhao, J. Baggs, J. G. Donahue, S. J. Hambidge, S. J. Jacobsen, N. P. Klein, A. L. Naleway, K. M. Zangwill and L. A. Jackson, *Am. J. Public Health*, 2009, **99**, S389–S397.
- 18 C. L. Ventola, *Pharmacol. Ther.*, 2016, **41**, 426–436.
- 19 S. K. Kurosky, K. L. Davis and G. Krishnarajah, *Vaccine*, 2016, **34**, 387–394.
- 20 A. Taddio, C. M. McMurtry, C. Logeman, V. Gudzak, A. de Boer, K. Constantin, S. Lee, R. Moline, E. Uleryk, T. Chera, N. E. MacDonald and B. Pham, *Vaccine*, 2022, **40**, 7526–7537.
- 21 H. Wang, L. Cui, Y. Luo, X. Zhou, R. Liu, Q. Chen, Y. Guan and Y. Zhang, *Biomater. Adv.*, 2022, **137**, 212812.
- 22 K. J. McHugh, R. Guarecuco, R. Langer and A. Jaklenec, *J. Controlled Release*, 2015, **219**, 596–609.
- 23 E. C. Gale, A. E. Powell, G. A. Roth, E. L. Meany, J. Yan, B. S. Ou, A. K. Grosskopf, J. Adamska, V. C. T. M. Picece, A. I. d'Aquino, B. Pulendran, P. S. Kim and E. A. Appel, *Adv. Mater.*, 2021, **33**, 2104362.
- 24 O. R. Brohlin, R. N. Ehrman, F. C. Herbert, Y. H. Wijesundara, A. Raja, A. Shahriverkevishahi,



- S. D. Diwakara, R. A. Smaldone and J. J. Gassensmith, *ACS Appl. Nano Mater.*, 2022, **5**, 13697–13704.
- 25 F. C. Herbert, S. S. Abeyrathna, N. S. Abeyrathna, Y. H. Wijesundara, O. R. Brohlin, F. Carraro, H. Amenitsch, P. Falcaro, M. A. Luzuriaga, A. Durand-Silva, S. D. Diwakara, R. A. Smaldone, G. Meloni and J. J. Gassensmith, *Nat. Commun.*, 2021, **12**, 2202.
- 26 S. Kumari, Y. H. Wijesundara, T. S. Howlett, M. Waliullah, F. C. Herbert, A. Raja, I. Trashy, R. A. Bernal and J. J. Gassensmith, *Proc. Natl. Acad. Sci. U. S. A.*, 2023, **120**, e2218247120.
- 27 W. Liang, P. Wied, F. Carraro, C. J. Sumby, B. Nidetzky, C.-K. Tsung, P. Falcaro and C. J. Doonan, *Chem. Rev.*, 2021, **121**, 1077–1129.
- 28 K. Liang, R. Ricco, C. M. Doherty, M. J. Styles, S. Bell, N. Kirby, S. Mudie, D. Haylock, A. J. Hill, C. J. Doonan and P. Falcaro, *Nat. Commun.*, 2015, **6**, 7240.
- 29 J. Yang and Y.-W. Yang, *Small*, 2020, **16**, 1906846.
- 30 S. Kumari, R. N. Ehrman and J. J. Gassensmith, *Matter*, 2023, **6**, 2570–2573.
- 31 M. A. Luzuriaga, F. C. Herbert, O. R. Brohlin, J. Gadhvi, T. Howlett, A. Shahrivarkevishahi, Y. H. Wijesundara, S. Venkitapathi, K. Veera, R. Ehrman, C. E. Benjamin, S. Popal, M. D. Burton, M. A. Ingersoll, N. J. De Nisco and J. J. Gassensmith, *ACS Nano*, 2021, **15**, 17426–17438.
- 32 M. A. Luzuriaga, R. P. Welch, M. Dharmawardana, C. E. Benjamin, S. Li, A. Shahrivarkevishahi, S. Popal, L. H. Tuong, C. T. Creswell and J. J. Gassensmith, *ACS Appl. Mater. Interfaces*, 2019, **11**, 9740–9746.
- 33 Y. H. Wijesundara, F. C. Herbert, O. Trashy, I. Trashy, O. R. Brohlin, S. Kumari, T. Howlett, C. E. Benjamin, A. Shahrivarkevishahi, S. D. Diwakara, S. D. Perera, S. A. Cornelius, J. P. Vizuet, K. J. Balkus, R. A. Smaldone, N. J. De Nisco and J. J. Gassensmith, *Chem. Sci.*, 2022, **13**, 13803–13814.
- 34 M. A. Luzuriaga, C. E. Benjamin, M. W. Gaertner, H. Lee, F. C. Herbert, S. Mallick and J. J. Gassensmith, *Supramol. Chem.*, 2019, **31**, 485–490.
- 35 C. Cheng, C. Li, X. Zhu, W. Han, J. Li and Y. Lv, *J. Biomater. Appl.*, 2019, **33**, 1373–1381.
- 36 Z. Teng, F. Hou, M. Bai, J. Li, J. Wang, J. Wu, J. Ru, M. Ren, S. Sun and H. Guo, *J. Mater. Chem. B*, 2022, **10**, 2853–2864.
- 37 M. A. Luzuriaga, A. Shahrivarkevishahi, F. C. Herbert, Y. H. Wijesundara and J. J. Gassensmith, *Wiley Interdiscip. Rev.: Nanomed. Nanobiotechnology*, 2021, **13**, e1735.
- 38 H. H. Tam, M. B. Melo, M. Kang, J. M. Pelet, V. M. Ruda, M. H. Foley, J. K. Hu, S. Kumari, J. Crampton, A. D. Baldeon, R. W. Sanders, J. P. Moore, S. Crotty, R. Langer, D. G. Anderson, A. K. Chakraborty and D. J. Irvine, *Proc. Natl. Acad. Sci. U. S. A.*, 2016, **113**, E6639–E6648.
- 39 K. M. Cirelli and S. Crotty, *Curr. Opin. Immunol.*, 2017, **47**, 64–69.
- 40 A. V. Boopathy, A. Mandal, D. W. Kulp, S. Menis, N. R. Bennett, H. C. Watkins, W. Wang, J. T. Martin, N. T. Thai, Y. He, W. R. Schief, P. T. Hammond and D. J. Irvine, *Proc. Natl. Acad. Sci. U. S. A.*, 2019, **116**, 16473–16478.
- 41 G. A. Roth, E. C. Gale, M. Alcántara-Hernández, W. Luo, E. Axpe, R. Verma, Q. Yin, A. C. Yu, H. Lopez Hernandez, C. L. Maikawa, A. A. A. Smith, M. M. Davis, B. Pulendran, J. Idoyaga and E. A. Appel, *ACS Cent. Sci.*, 2020, **6**, 1800–1812.
- 42 K. M. Cirelli, D. G. Carnathan, B. Nogal, J. T. Martin, O. L. Rodriguez, A. A. Upadhyay, C. A. Enemu, E. H. Gebru, Y. Choe, F. Viviano, C. Nakao, M. G. Pauthner, S. Reiss, C. A. Cottrell, M. L. Smith, R. Bastidas, W. Gibson, A. N. Wolabaugh, M. B. Melo, B. Cossette, V. Kumar, N. B. Patel, T. Tokatlian, S. Menis, D. W. Kulp, D. R. Burton, B. Murrell, W. R. Schief, S. E. Bosinger, A. B. Ward, C. T. Watson, G. Silvestri, D. J. Irvine and S. Crotty, *Cell*, 2019, **177**, 1153–1171.e28.
- 43 B. S. Ou, O. M. Saouaf, J. Baillet and E. A. Appel, *Adv. Drug Delivery Rev.*, 2022, **187**, 114401.
- 44 N. J. Kräutler, D. Suan, D. Butt, K. Bourne, J. R. Hermes, T. D. Chan, C. Sundling, W. Kaplan, P. Schofield, J. Jackson, A. Basten, D. Christ and R. Brink, *J. Exp. Med.*, 2017, **214**, 1259–1267.
- 45 N. K. Maddigan, A. Tarzia, D. M. Huang, C. J. Sumby, S. G. Bell, P. Falcaro and C. J. Doonan, *Chem. Sci.*, 2018, **9**, 4217–4223.
- 46 L. Tong, S. Huang, Y. Shen, S. Liu, X. Ma, F. Zhu, G. Chen and G. Ouyang, *Nat. Commun.*, 2022, **13**, 951.
- 47 F. Carraro, J. D. Williams, M. Linares-Moreau, C. Parise, W. Liang, H. Amenitsch, C. Doonan, C. O. Kappe and P. Falcaro, *Angew. Chem., Int. Ed.*, 2020, **59**, 8123–8127.
- 48 M. D. R. Weber, T. L. Baker, B. Dao, C. Kwon and F. Tian, *Cryst. Growth Des.*, 2020, **20**, 2305–2312.
- 49 S. Kumari, T. S. Howlett, R. N. Ehrman, S. Koirala, O. Trashy, I. Trashy, Y. H. Wijesundara and J. J. Gassensmith, *Chem. Sci.*, 2023, **14**, 5774–5782.
- 50 M. Hoop, C. F. Walde, R. Riccò, F. Mushtaq, A. Terzopoulou, X.-Z. Chen, A. J. deMello, C. J. Doonan, P. Falcaro, B. J. Nelson, J. Puigmartí-Luis and S. Pané, *Appl. Mater. Today*, 2018, **11**, 13–21.
- 51 J. Lin, L. Huang, H. Ou, A. Chen, R. Xiang and Z. Liu, *RSC Adv.*, 2021, **11**, 21414–21425.
- 52 M. Kool, K. Fierens and B. N. Lambrecht, *J. Med. Microbiol.*, 2012, **61**, 927–934.
- 53 H. HogenEsch, *Front. Immunol.*, 2013, **3**.
- 54 D. L. Portuondo, A. Batista-Duharte, L. S. Ferreira, C. R. de Andrade, C. Quinello, D. Téllez-Martínez, M. L. de Aguiar Loesch and I. Z. Carlos, *Vaccine*, 2017, **35**, 4430–4436.
- 55 N. Goto, H. Kato, J.-i. Maeyama, K. Eto and S. Yoshihara, *Vaccine*, 1993, **11**, 914–918.
- 56 W. Jiang, B. Y. S. Kim, J. T. Rutka and W. C. W. Chan, *Nat. Nanotechnol.*, 2008, **3**, 145–150.
- 57 K. Donaldson and C. A. Poland, *Curr. Opin. Biotechnol.*, 2013, **24**, 724–734.
- 58 J. I. Andorko, K. L. Hess and C. M. Jewell, *Arch. Aesthetic Plast Surg*, 2015, **17**, 323–338.
- 59 T. J. Moyer, A. C. Zmolek and D. J. Irvine, *J. Clin. Investig.*, 2016, **126**, 799–808.
- 60 N. Tyagi, Y. H. Wijesundara, J. J. Gassensmith and A. Popat, *Nat. Rev. Mater.*, 2023, **8**, 701–703.
- 61 I. Wessels, M. Maywald and L. Rink, *Nutrients*, 2017, **9**.



- 62 A. S. Prasad, *Mol. Med.*, 2008, **14**, 353–357.
- 63 M.-K. Ko, H. W. Kim, S. H. Park, J.-H. Park, S.-M. Kim and M. J. Lee, *Virus Res.*, 2023, **335**, 199189.
- 64 A. Collins, P. Møller, G. Gajski, S. Vodenková, A. Abdulwahed, D. Anderson, E. E. Bankoglu, S. Bonassi, E. Boutet-Robinet, G. Brunborg, C. Chao, M. S. Cooke, C. Costa, S. Costa, A. Dhawan, J. de Lapuente, C. D. Bo', J. Dubus, M. Dusinska, S. J. Duthie, N. E. Yamani, B. Engelward, I. Gaivão, L. Giovannelli, R. Godschalk, S. Guilherme, K. B. Gutzkow, K. Habas, A. Hernández, O. Herrero, M. Isidori, A. N. Jha, S. Knasmüller, I. M. Kooter, G. Koppen, M. Kruszewski, C. Ladeira, B. Laffon, M. Larramendy, L. L. Hégarat, A. Lewies, A. Lewinska, G. E. Liwszyc, A. L. de Cerain, M. Manjanatha, R. Marcos, M. Milić, V. M. de Andrade, M. Moretti, D. Muruzabal, M. Novak, R. Oliveira, A.-K. Olsen, N. Owiti, M. Pacheco, A. K. Pandey, S. Pfuhler, B. Pourrut, K. Reisinger, E. Rojas, E. Rundén-Pran, J. Sanz-Serrano, S. Shaposhnikov, V. Sipinen, K. Smeets, H. Stopper, J. P. Teixeira, V. Valdiglesias, M. Valverde, F. van Acker, F.-J. van Schooten, M. Vasquez, J. F. Wentzel, M. Wnuk, A. Wouters, B. Žegura, T. Zikmund, S. A. S. Langie and A. Azqueta, *Nat. Protoc.*, 2023, **18**, 929–989.
- 65 T. Hägglöf, M. Cipolla, M. Loewe, S. T. Chen, L. Mesin, H. Hartweger, M. A. ElTanbouly, A. Cho, A. Gazumyan, V. Ramos, L. Stamatatos, T. Y. Oliveira, M. C. Nussenzweig and C. Viant, *Cell*, 2023, **186**, 147–161.
- 66 J. H. Lee, H. J. Sutton, C. A. Cottrell, I. Phung, G. Ozorowski, L. M. Sewall, R. Nedellec, C. Nakao, M. Silva, S. T. Richey, J. L. Torre, W.-H. Lee, E. Georgeson, M. Kubitz, S. Hodges, T.-M. Mullen, Y. Adachi, K. M. Cirelli, A. Kaur, C. Allers, M. Fahlberg, B. F. Grasperge, J. P. Dufour, F. Schiro, P. P. Aye, O. Kalyuzhnyi, A. Liguori, D. G. Carnathan, G. Silvestri, X. Shen, D. C. Montefiori, R. S. Veazey, A. B. Ward, L. Hangartner, D. R. Burton, D. J. Irvine, W. R. Schief and S. Crotty, *Nature*, 2022, **609**, 998–1004.
- 67 N. S. De Silva and U. Klein, *Nat. Rev. Immunol.*, 2015, **15**, 137–148.
- 68 G. D. Victora and M. C. Nussenzweig, *Annu. Rev. Immunol.*, 2012, **30**, 429–457.
- 69 M. Heidary, V. H. Kaviar, M. Shirani, R. Ghanavati, M. Motahar, M. Sholeh, H. Ghahramanpour and S. Khoshnood, *Front. Microbiol.*, 2022, **13**, 927306.

